

# A Review on the Analysis and Experiment of Fluid Flow and Mixing in Micro-Channels

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## Abstract

The studies with respect to micro-channels and micro-mixers are expanding in many dimensions. Most significant area of micro-mixer study is the flow analysis in various micro-channel configurations. The flow phenomena in micro-channel devices are quite different from that of the macro-scale devices. An attempt is made here to review the important recent literature available in the area of micro-channel flow analysis and mixing. The topics covered include the physics of flow in micro-channels and integrated simulation of the micro-channel flow. Also, the flow control models and electro-kinetically driven micro-channel flows are dealt in detail. A survey of important numerical methods, which are currently popular for micro-channel flow analysis, is carried out. Different options for mixing in micro-channels are provided, in sufficient detail.

*Keywords:* Micro-channel, Mixing, Flow Analysis, Review

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## 1. Introduction

The phenomenon of mixing is so fundamental, that we face it everywhere in our daily life. The applications of mixing range from chemical reactions in industries to environmental studies with respect to pollution. The importance of mixing in micro-scale applications can never be under-estimated. Especially, the successful operation of new micro-devices, such as the lab-on-a-chip or  $\mu$ TAS, very much depends on the efficient mixing process of various fluid constituents.

Unlike the macro-scale applications, the micro-channels provide new challenges for carrying out the mixing operation effectively, the foremost reason being the low Reynolds number value of the micro-

channel flow. Also, the small and intricate dimensions of the flow-conduit in micro-channels do not easily permit any mechanical stirring arrangement, which can help to enhance the mixing.

By definition, micro-channels are flow domains having their internal dimensions within the range of 1mm and 1 $\mu$ m. Due to various advantages that micro-channels offer, their applications range from compact heat exchangers to MEMS devices that are used for biological and chemical analysis. At present, micro-channels are used to transport and mix biological materials such as proteins, DNA, cells, etc. or to send chemical samples from one place to the other. A comprehensive coverage about micro-channel applications and the important aspects of the micro-channel flow are provided by Gad-el-Hak (2006).

This paper presents a review on the micro-channel flow and mixing. A highlight about modeling of micro-channel flows is elaborated in Sec. 2. Different

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channel configurations and fluid models are discussed here. A note on the experiments with micro-channels is given in Sec. 3. In the micro-scales, fluid stirring becomes one of the most crucial factors in the design and operation of micro-devices. Explanations about the electro-kinetic transport and mixing in micro-channels are presented in Sec. 4 and Sec. 5, respectively.

## 2. Modeling Micro-Channel Flow

The physics of flow and energy transfer in micro-channel devices is found to be quite different from that of macro-scale devices. A well known example for this is the failure of Fourier law to predict the thermal conductivity of micro-structures (Gen, 2001). Luckily, the potential interaction distance is very small in typical liquid systems and the continuum description is valid for most micro systems, as well. Fluid flow in micro-channels typically requires higher pressure differences and the flow rates are very small. Thus micro-channel flow phenomena often demand a different way of analysis and special numerical tools.

The understanding of the unconventional physics involved in the manufacture and operation of small devices is crucial for designing, optimizing, fabricating and utilizing the improved MEMS. In dealing with the flow through micro-devices, the selection of physical and mathematical models, boundary conditions and solution procedure are quite critical. It is well known that the surface effects are going to dominate in micro-devices (Knight, 1999). The million-fold increase of surface area relative to the mass of the minute devices (per unit volume), substantially affects the transport of mass, momentum and energy through the surface.

A major difficulty in connection with the micro-channel analysis is the geometrical complexity of the flow domain. Numerous designs of micro-channels have been proposed, including T and H shaped channels, zigzag shaped channels, 2D and 3D serpentine channels and multi-laminators. The T-sensor designed by Weigle and Yager (1999) for implementation of assays in micro-channels is quite popular. In this design a reference stream, a detection stream and a sample stream are introduced through multiple T junctions into a common channel. Differential diffusion rates are also fundamental to the design of H-filter, used to separate components (Sculte et al., 2000). Splitting the streams and re-layering increases

the interfacial area which promotes mixing. This layering approach was implemented by Branbjerg et al. (1996). By adding complexity to the flow field, this has good potential to increase the amount of mixing between the streams. The three dimensional serpentine channel proposed by Liu et al. (2000) was designed to introduce chaotic advection into the system and further enhance mixing.

### 2.1 Integrated simulation of micro-channel flow

For a larger class of flows, Navier-Stokes equations based on the continuum assumption are adequate to model the fluid behavior. Continuum approximation implies that the mean free path of the molecules,  $\lambda$ , in a gas is much smaller than the characteristic length,  $L$ . That is, the Knudsen number,  $Kn = \lambda / L$ , has to be very small ( $\ll 1$ ). However, there are special cases in micro-channel flow, that do not satisfy this condition. The various flow regimes and suitable fluid models are shown in Table 1 (Arkilic et al., 1997).

As shown in this table, Navier-Stokes equation together with Boltzmann equation describes the flow in all regimes. For the accurate prediction of the flow parameters in micro-channels, it is very important that a suitable numerical tool is used for the analysis. Often in the literature it is found that the standard Navier-Stokes solvers are extended to yield solution for micro-channel flow parameters. While doing so, one should be very careful to incorporate the additional considerations with respect to the micro-channels. Along with the Navier-Stokes solvers,

Table 1. Flow regimes & fluid models for micro-channels.

Knudsen Number	Fluid Model
$Kn \rightarrow 0$ (continuum, no molecular diffusion)	Euler equations with slip-boundary conditions
$Kn \leq 10^{-3}$ (continuum, with molecular diffusion)	Navier-stokes equations with no-slip-boundary conditions
$10^{-3} \leq Kn \leq 10^{-1}$ (continuum-transition)	Navier-stokes equations with slip-boundary conditions
$10^{-1} \leq Kn \leq 10$ (transition)	Burnett equations with slip-boundary conditions Moment equations DSMC Lattice Boltzmann
$Kn > 10$ (free molecular flow)	Collisionless Boltzmann DSMC

molecular based numerical simulation methods (for example, the lattice Boltzmann method) for liquid and gas micro-flows are also being tried.

Many diverse processes with disparate spatial and temporal scales are involved in the full-system simulation of micro-channels. Fluidic devices often require full simulation of the individual components. This is particularly true for new designs, for which the lumped models and continuum approximations are inappropriate. To develop a system level simulation that is sufficiently accurate and robust, all processes involved must be simulated at a comparable degree of accuracy and integrated seamlessly.

Liquid and gas flows in micro-devices are characterized by low Reynolds number and unsteady nature. The Reynolds number values are typically of order one or less in channels with heights in the sub-millimeter range (Ho and Tai, 1998). The unsteadiness is due to the external excitation from a moving boundary or an electric field, often driven by high-frequency oscillators (Freeman et al., 1998). The domain is largely three dimensional and geometrically complex, consisting of large aspect ratio components, abrupt expansions and rough boundaries. In addition, micro-devices interact with larger devices, resulting in fluid flow going through disparate regimes. Accurate and efficient simulation of micro-flows should take into account the above factors. For example, the significant geometric complexity of MEMS flows suggests that finite elements and finite volumes are more suitable than finite differences for efficient discretization (Ye et al., 1999). A particularly promising approach applied recently for MEMS flow analysis makes use of mesh-less and mesh-free approaches as explained by Aluru (1999).

In coupled domain problems, such as flow-structure or structure-electric (or a combination of both), there are significant disparities in temporal and spatial scales. These disparities, in turn, imply that multiple grids and heterogeneous time-stepping algorithms may be needed for discretization, leading to very complicated (and consequently), computationally prohibitive simulation algorithms. Possible construction of low-order dynamical models could be achieved by projecting the results of detailed numerical simulations onto spaces spanned by a very small number of degrees of freedom; the so-called non-linear macro-modeling approach (Senturia et al., 1997).

Construction of macro-models is not always possible, and this lack of simplified models for the many and

diverse components of micro-systems makes system level simulation a challenging task. As there is enough progress in model development of electronic components, now considerable attention needs to be focused on models for non-electronic components. An illustration on the full simulation of fluidic system, which involves interaction with adjacent structures, is presented in Fig. 1. This is an anemometer-type flow sensor, which is made up of a heating element and two sensing elements (Rasmussen and Zaghoul, 1999). The temperature difference between the sensors is used to measure the flow parameters.

## 2.2 Molecular based micro-fluidic simulation

Since micro-channels have very small volume-to-surface ratios, the surface forces are more dominant

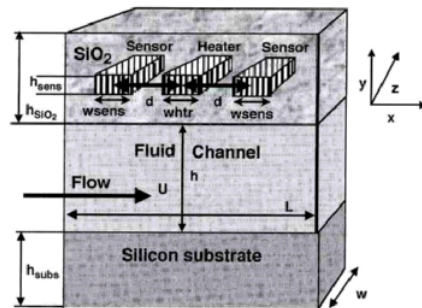


Fig. 1. Structure of an anemometer type flow sensor (Rasmussen and Zaghoul, 1999).

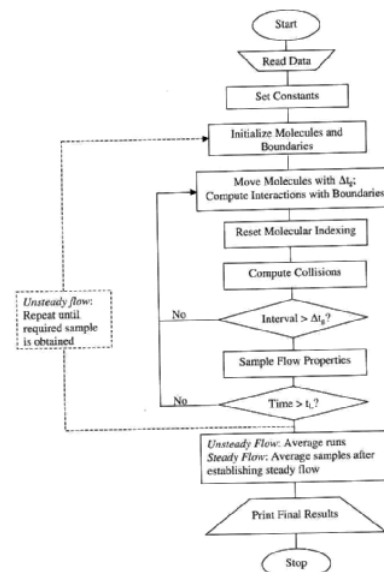


Fig. 2. Steps for a typical DSMC method.

than the body forces in such small scales. The origin of the surface forces is atomistic and based on the short-ranged van der Waals forces and longer ranged electrostatic or Coulombic forces. Although molecular simulation based approach for understanding fluid forces on surfaces is fundamental in nature, it is very difficult to apply the same to engineering problems, due to the vast number of molecules involved in the analysis. Also, the fundamental simulation approaches, from a microscopic point of view, differ for liquid and gas flows. Examples for molecular based micro-scale transport modeling are the Direct Simulation Monte Carlo (DSMC) algorithm and the Lattice Boltzmann Method (LBM).

The DSMC method was invented by Bird (1994) and several review articles are currently available (for example, Oran et al., 1998). This method is based on splitting the molecular motion and inter-molecular collisions by choosing a time step, less than the mean collision time and evolution of this molecular process in space and time. For efficient numerical implementation, the space is divided into cells (which are proportional to the mean free path,  $\lambda$ ) similar to the finite-volume method. The basic steps of the DSMC algorithm, as explained by Oran et al. (1998), is shown in Fig. 2. It should be noted that, irrespective of its attractions, there are several possible limitations and error sources within the DSMC method.

Micro-scale thermal/fluidic transport in the entire Knudsen regime ( $0 \leq Kn < \infty$ ) is governed by the Boltzmann equation (BE). This equation describes the evolution of a velocity distribution function by molecular transport and binary intermolecular collisions; which is given in the following form (Bird, 1994) for the case of a simple dilute gas domain:

$$\frac{\partial n f}{\partial t} + c \frac{\partial n f}{\partial x} + F \frac{\partial n f}{\partial c} = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} n^2 (f^* f_1^* - f f_1) c_r \sigma d\Omega dc_1$$

where  $f$  is the velocity distribution function,  $n$  the number density,  $c$  the molecular velocity,  $F$  the external force per unit mass,  $c_r$  the relative speed of class  $c$  molecules with respect to class  $c_1$  molecules, and  $\sigma$  the differential collision cross section. The Lattice Boltzmann method is based on the solution of this equation on a previously defined lattice structure with simplistic molecular collision rules. A good review article on LBM is given by Chen and Doolen (1998). The LBM can be viewed as a

special finite differencing scheme for the kinetic equation of the discrete velocity distribution function, and it is possible to recover the Navier-Stokes equations from the discrete lattice Boltzmann equation with sufficient lattice symmetry (Frish et al., 1986).

During the last decade, LBM has been developed as an alternative and versatile numerical simulation method in computational fluid dynamics (CFD). LBM has relatively simple algorithms, and it has the potential for obtaining an easier solution for fluid flow problems instead of solving the Navier-Stokes equations (Qian et al., 1992). A flow chart giving step by step procedure of the free energy model in LBM is shown in Fig. 3. Many complicated CFD problems (multi-phase flows, multi-component flows, turbulent flows, etc.) have been simulated by researchers in the recent past, using LBM. It is easier to apply LBM to fluid applications involving interfacial dynamics and complex boundaries (Sukop and Thorne, 2006). Another useful application of the LBM is for granular flows, which can be expanded to include flow through micro-filtering systems (Angelopoulos et al., 1998). An interesting numerical simulation of two-phase flow within a micro-channel using free energy model of the LBM is carried out recently by Li and Suh (2006). Of course, LBM is not free of disadvantages. Firstly, implementation of boundary conditions

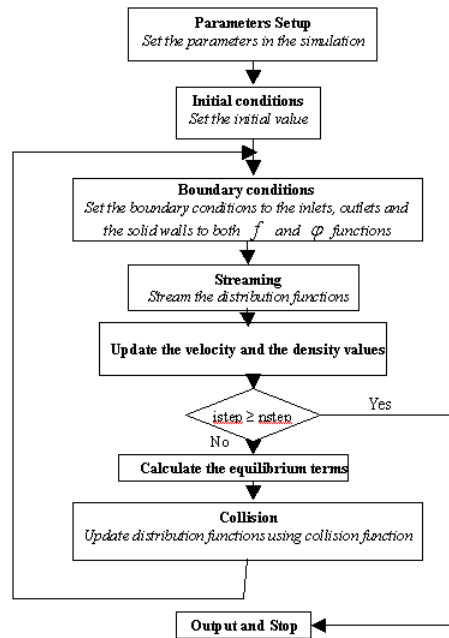


Fig. 3. Free-energy model based LBM algorithm.

is not straightforward as in the Navier-Stokes solvers, because the primary variable is the distribution function not the velocity field itself. Secondly, since LBM is basically based on the compressible-fluid assumption, the solutions contain the compressible effect anyhow, and so when the exact incompressibility should be a very important restriction, LBM is not suitable. These are currently the main issues among the researchers involved in the development of LBM techniques.

### 3. Experiments with micro-channel flows

During the last decade and more, numerous reports have appeared in the literature about experiments with micro-channels. The experimental study of micro-channel flow is plagued by many discrepancies, owing to the difficulty in conducting micro-scale measurements. Despite the fundamental simplicity of laminar flow in straight ducts, it often failed to reveal the expected relationship between the friction factor and Reynolds number with respect to micro-channels. Table 2 gives a summary of some experiments conducted by various researchers to investigate the behavior of fluid flow over a large range of Reynolds numbers, geometries and experimental conditions. Most of these experiments are aimed at determining the friction factor with respect to micro-channels. The inconsistencies observed by these experiments demonstrate the need for detailed velocity measurements in order to elucidate potential micro-scale effects and mechanisms in these channels.

#### 3.1 Velocity measurement in micro-channels

Measurement of velocity in micro-channels has been carried out using bulk flow, point-wise or field measurements. Each of these techniques has certain advantages making it more suitable to provide a specific type of flow-field information. The majority of flow resistance data to date has been obtained through the use of bulk flow measurements. It is the most simple and cheap method of flow measurement without any optical access and seeding. The point-wise and field velocity measurements were essentially done by micro-PIV (Particle Image Velocimetry), first made by Santiago et al. (1998).

Alternate visual methods applied to micro-channel velocity measurements have been demonstrated by numerous researchers (for example, Brody et al., 1996). Molecular Tagging Velocimetry (MTV) was

Table 2. Micro-channel experiments.

Channel Description		Reynolds	Reference
Shape	Size	Number Range	
Trapezoidal/ Rectangular	$d = 50\text{--}56 \mu\text{m}$ $w = 287\text{--}320 \mu\text{m}$ $l = 1\text{cm}$	200~600	Tuckerman & Pease (1981)
Trapezoidal or U-shaped	$d = 28\text{--}65 \mu\text{m}$ $w = 40\text{--}150 \mu\text{m}$ $l = 7.6\text{--}40.3\text{mm}$	200~ 15,000	Wu & Little (1983)
Rectangular/ Trapezoidal	$d = 0.48\text{--}38.7 \mu\text{m}$ $w = 55\text{--}115 \mu\text{m}$ $l = 10.2\text{--}10.9 \text{mm}$	<<1-80 (approx.)	Pfahler et al. (1991)
Rectangular	$d = 100\text{--}300 \mu\text{m}$ $w = 200\text{--}400 \mu\text{m}$ $l = 50 \text{mm}$	50~ 4,000	Peng et al. (1994)
Trapezoidal	$d = 20\text{--}40 \mu\text{m}$ $w = 40\text{--}150 \mu\text{m}$ $l = 11.7 \text{mm}$	17~126	Wilding et al (1994)
Circular Trapezoidal & Triangular	$d = 8\text{--}42 \mu\text{m}$ $d = 13.4\text{--}46 \mu\text{m}$ $w = 35\text{--}110 \mu\text{m}$ $l = 2.5\text{--}10 \text{mm}$	<1.2 (approx.)	Jiang et al. (1995)
Trapezoidal	$d = 27\text{--}63 \mu\text{m}$ $w = 100\text{--}1000 \mu\text{m}$ $l = 12\text{--}36 \text{mm}$	<600	Flockhart & Dhariwal (1998)
Rectangular (channel array)	$d = 30 \mu\text{m}$ $w = 600 \mu\text{m}$ $l = 3 \text{mm}$	1~18	Papautsky et al. (1999a)
Rectangular (channel array)	$d = 22.71\text{--}26.35 \mu\text{m}$ $w = 150\text{--}600 \mu\text{m}$ $l = 7.75 \text{mm}$	0.001~10	Papautsky et al. (1999b)
Trapezoidal	$d = 28\text{--}114 \mu\text{m}$ $w = 148\text{--}523 \mu\text{m}$ $l = 28 \text{mm}$	10~1,450	Qu et al. (2000)
Circular	$d = 3\text{--}81 \mu\text{m}$	30~ 20,000	Choi et al. (1991)
Circular	$d = 19\text{--}102 \mu\text{m}$	250~ 20,000	Yu et al. (1995)
Circular	$d = 50\text{--}254 \mu\text{m}$	upto 2,500	Mala & Li (1999)
Circular	$d = 75\text{--}242 \mu\text{m}$	50~2,500	Sharp et al. (2000)

$d$  =depth/diameter;  $w$  =width;  $l$  =length

adapted to micro-scale by Webb and Maynes (1999), where velocity profiles were obtained in circular tubes with  $d = 705 \mu\text{m}$  and  $\text{Re} = 800$  to 2200. Micro-PIV and Nuclear Magnetic Resonance (NMR) techniques have also been applied to the measurement of velocities in electro-osmotic flow (Cummings et al., 1999). An adaptation of Laser Doppler Anemometry

(LDA) techniques to micro-scale flows was demonstrated by Tieu et al. (1995), with point-wise data obtained in a 175 μm channel.

**4. Electro-kinetics in micro-fluidics**

Another important aspect which has to be taken care of, in the case of micro-channel flow and mixing analysis, is the electro-kinetic effect. Electro-kinetics is a general term describing the phenomena, which involve interaction between solid surfaces, ionic solutions and macroscopic electric fields. Both electro-phoresis and electro-osmosis phenomena need to be considered in micro-channel flow analysis. The fluid pumping that occurs in a micro-capillary, when an electric field is applied along the axis of the capillary is a typical example of the latter. Electro-kinetic transport refers to the combination of electro-osmotic and electro-phoretic transports. A detailed review of electro-kinetic transport is available in a recent publication by Li (2004).

**4.1 Electric double layer**

The interactions between charged particles and electric fields often involve the electric double layers (EDL), formed at liquid/solid interfaces. The EDL is formed due to the presence of the static charges on the solid surfaces. Generally, a dielectric surface acquires charges when it is in contact with a polar medium or by chemical reaction, ionization or ion absorption. A schematic view of this is shown in Fig. 4. In this figure,  $\Psi$  is the electric potential,  $\Psi_0$  the surface electric potential,  $\zeta$  the zeta potential and  $y'$  distance measured from the wall. When the solid surface is in contact with a polar medium, a net electric potential is generated on the surface. Due to this surface electric potential, positive ions in the liquid are attracted to the wall, whereas the negative ions are repelled from the wall. This results in the redistribution of the ions close to the wall, keeping the bulk of the liquid far away from the wall electrically neutral. The distance from the wall, where the electric potential energy is equal to the thermal energy, is known as the Debye length ( $\lambda$ ), and this zone is known as the EDL. The electric potential distribution within the fluid is described by the Poisson-Boltzmann equation:

$$\nabla^2(\Psi / \zeta) = \frac{-4\pi h^2 \rho_e}{D\zeta} = \beta \sinh(\alpha \Psi / \zeta)$$

Here  $\alpha$  is the ionic energy parameter given as:

$$\alpha = ez\zeta / k_b T$$

Parameter  $\beta$  is as shown below:

$$\beta = (\omega h)^2 / \alpha \quad \text{where} \quad \omega = 1/\lambda = \sqrt{\frac{2 n_0 e^2 z^2}{\epsilon k_b T}}$$

The other symbols in these equations are  $\rho_e$ : net charge density,  $e$ : electron charge,  $z$ : valance,  $k_b$ : Boltzmann constant,  $T$ : temperature, and  $h$ : characteristic length.

**4.2 Electro-osmotic flow**

Electro-osmosis is the bulk movement of aqueous solution past a stationary solid surface, due to an externally applied electric field. Electro-osmosis requires the existence of a charged double layer at the solid-liquid interface. The electro-osmotic flow is created by applying the electric field in the stream-wise direction, where this electric field ( $\mathbf{E}$ ) interacts with the electric charge distribution ( $\rho_e$ ) and creates an electro-kinetic body force on the fluid. The ionized incompressible fluid flow with electro-osmotic body forces is governed by the incompressible Navier-Stokes equation:

$$\rho_f \left( \frac{\partial \mathbf{V}}{\partial t} + (\mathbf{V} \cdot \nabla) \mathbf{V} \right) = -\nabla P + \mu \nabla^2 \mathbf{V} + \rho_e \mathbf{E}$$

Here  $\rho_f$ ,  $\mathbf{V}$  and  $P$  are the fluid density, velocity vector and pressure, respectively. Based on these continuum based equations, various researchers have developed numerical models to simulate electro-kinetic effects in micro-devices (Yang et al., 1998).

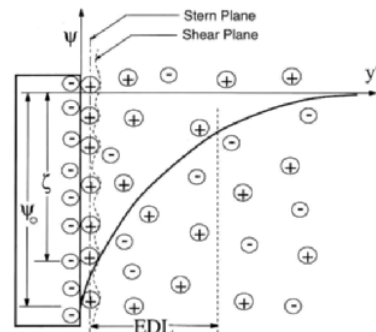


Fig. 4. EDL next to a negatively charged solid surface.

Recently, there is renewed interest in the field of electro-osmotic flow analysis, considering its importance in the micro-channel applications. Qian and Bau (2005) carried out a theoretical investigation of electro-osmotic flows with chaotic stirring in rectangular cavities. Earlier, they (Qian and Bau, 2002) had explained about a new chaotic electro-osmotic stirrer principle. A study about electro-osmotic flow in micro-channels with arbitrary geometry and arbitrary distribution of wall charge was done by Xuan and Li (2005). They have found that the wall charge affects significantly the electro-osmotic flow while the channel geometry does not.

### 4.3 Electrophoresis

Electrophoresis describes the motion of a charged particle submerged in a fluid under the action of an applied electric field. Considering the case of a charged dye molecule, the electrophoretic velocity,  $U$ , of the dye is described by the Helmholtz-Smoluchowski equation (Probstein, 1994):

$$U = \frac{\epsilon \zeta_{EP} E_x}{\mu}$$

The electro-osmotic zeta potential,  $\zeta_{EO}$  is a property of the capillary surface while the electrophoretic zeta potential,  $\zeta_{EP}$  is a property of the charged dye and, in general these two zeta potentials will not be equal.

## 5. Mixing in micro-channels

### 5.1 Passive and active micro-mixers

The importance of mixing in micro-channels can never be under-estimated. Efficient micro-mixers are vital for the successful operation of bio-fluid systems. The performance of these devices depends largely on the rapid and efficient mixing of different fluids. This has to be achieved, in spite of the difficulties put forth by the fundamental physics of flow in narrow channels, with high viscosity and low Reynolds number values. Various alternatives are being tried with the aim of reaching the final goal, which is instantaneous mixing (Liu et al., 2000). Also, the effect of fluid mixing needs to be considered in many other micro-systems, like fluid control and pumping systems, where the major aim may be reducing the pressure drop (Koch et al., 2000).

The application of micro-mixers range from the modern sample preparation for the 'lab on a chip' devices to traditional mixing tanks for purposes such as, blending, reaction, gas absorption, foaming and emulsification (Ehrfeld, 2000; Fletcher et al., 2002; Pennemann et al. 2004). The flow rates in micro-mixers range from as low as, less than 1  $\mu$ l/h to more than 1 ml/h. By-and-large, the micro-flow and mixing is typically done in the laminar regime at very low Reynolds number values (Schonfeld et al., 2004).

In micro-fluidic devices, the mixing relies solely on molecular inter-diffusion (Graveson et al., 1993), due to the absence of turbulence. Diffusive mixing can be optimized by maximization of the constitutive factors like the diffusion coefficient, interfacial surface area and the gradient of species concentration. Basically, 'the art of micro-mixing' translates to an efficient maximization of the interfacial surface area and concentration gradient. Also, convective mixing is commonly employed in the mixing devices.

Mixing in micro-scale is performed either by energy input from the exterior (active mixing) or by the flow energy due to pumping action/hydrostatic potential (passive mixing). Tables 3 and 4 give the various options available in these categories (respectively), and the corresponding literature references.

Table 3. Active mixing by external energy input.

External energy source	Reference
Ultrasound	Yang et al. (2001)
Acoustically induced vibrations	Liu et al. (2003)
Electro-kinetic instabilities	Oddy et al. (2001)
Variation of pumping capacity	Glasgow&Aubry(2003)
Electro-wetting induced droplets	Palk et al. (2003)
Piezo-electric vibrating membranes	Woiass et al (2000)
Magneto-hydrodynamic action	West et al. (2002)
Small impellers	Lu et al. (2001)
Integrated micro-valves/pumps	Voldman et al. (1998)

Table 4. Passive mixing by pumping power.

Principle	Reference
Inter-digital multi-lamellae arrangement	Lob et al (2004)
Split-and-recombine concepts	Schonfeld et al. (2004)
Chaotic mixing by eddy formation and folding	Jiang et al. (2004)
Nozzle injection in flow	Miyake et al. (1993)
Collision of jets	Werner et al. (2002)
Specialties like the Coanda-effect	Hong et al. (2001)

Some typical generic micro-structure designs employed for passive mixing includes the following (Lowe et al., 2000).

- (i) T and Y flow configurations
- (ii) Inter-digital and bifurcation flow distribution
- (iii) Focusing structures for flow compression
- (iv) Repeated flow division and recombination
- (v) Flow obstacles within micro-channels
- (vi) Meander-like or zig-zag channels
- (vii) Multi-hole plates
- (viii) Tiny nozzles
- (ix) Specialty flow arrangements

Numerical and experimental investigations on liquid mixing in static micro-mixers were reported by Engler et al. (2004). Their overall aim was to develop basic rules for the design and implementation of successful micro-mixers. Electro-hydrodynamic flow generated by the motion of charge carriers in an electric field was investigated for rapid mixing in micro-channel devices by Tsouris et al. (2003). “T” geometry channels ranging from 40 to 110  $\mu\text{m}$  in width and 30 to 60  $\mu\text{m}$  in depth was used to contact two miscible fluids, such as alcohols in this study. Electro-kinetically driven active micro-mixers utilizing zeta potential variation induced by field effect is investigated by Lee et al. (2004). The development of such electro-kinetically driven micro-mixer could be crucial for  $\mu\text{TAS}$  devices. More recently, Sounart et al. (2005) describes about the frequency-dependent electro-static actuation in micro-fluidic MEMS. Their analysis demonstrates the importance of native oxide on silicon actuator response, and suggests that the actuator frequency can be shifted by controlling the thickness of the oxide.

Hessel et al. (2004) presented the vast literature survey on the micro-mixing of miscible fluids in the chemical engineers’ point of view.

### 5.2 Mixing by chaotic advection

The chaotic stirring is a best suited principle for mixing in micro-channels, owing to the existence of low Reynolds number values. Chaotic advection is basically meant to effect stirring in the laminar flow. The salient feature of chaotic advection in the present context is the exponential growth of the interfacial area accompanied by a corresponding reduction of the striation thickness. A comprehensive coverage on the principle of chaotic advection and its mathematical descriptions is given in the book by Ottino (1989).

There are many other interesting publications on this topic, available in the literature (for example, Suh, 1991).

Steady, three-dimensional chaotic flows have been successfully used for micro-mixing in several contexts (see Jen, et al., 2003 and Jiang et al., 2004). The first publication on chaotic advection by micro-mixers rely on placing micro-structured objects within the flow passage on one side of the micro-channels (Stroock et al., 2002). A much simpler channel design, based solely on alternatively curved micro-channels, has been proposed by Schonfeld and Hardt (2003). The laminar flow patterns and the mixing performance of the comparable mixers with diagonal or asymmetric grooves was investigated and quantified by Kang and Kwon (2004). More recently, Heo and Suh (2005) have studied the enhancement of stirring in a straight channel at low Reynolds numbers with various block arrangement at different heights and angles. The Lyapunov exponents were computed and it was found that the stirring gets enhanced considerably at larger block heights. Both theoretical and experimental investigations with respect to a magneto-hydrodynamic (MHD) stirrer that exhibits chaotic advection were reported by Yi et al. (2002). Since this device has no moving parts, it is especially suitable for micro-fluidic applications, where efficient stirring is essential.

### 5.3 Mixing efficiency

The easiest method for judging the mixing efficiency in micro-mixer structures is by flow visualization, which is done using dilution-type experiments (Hassel et al., 2003). Reaction-type experiments underlay the mixing with very fast reaction so that mixed region spontaneously indicate the result of the reaction. Roessler and Rys (2001) introduced two parallel reactions (competitive reactions) which develop differently under varying pH, solvent, etc. This in turn, can be used as a measure of the mixing efficiency. By properly designing the micro-channel manifold, one can accomplish parallel and serial electro-kinetic mixing using a simple voltage-control circuit (Jacobson et al., 1999). Mixing in micro-fluidic devices typically occurs by the interplay of molecular diffusion and pressure-driven convection (dispersion) in the laminar regime. Mixing rates can be enhanced by using the principle of flow lamination (Bessoth et al., 1999),



whereby the streams are divided into  $n$  laminae with widths  $l/n$  of the original channel. This can result in faster mixing by a factor of  $n^2$ .

Concentrations are easily accessible by photometric or fluorescence measurements. Besides using photometric techniques, vibrational analysis such as Infrared and Raman can be used following the mixing course in a micro-mixer device (Loebbecke et al., 2002). To quantitatively represent the composition uniformity, Lu et al. (2001) and Bakker et al. (2000) used the coefficient of variation, COV, which is the ratio of the standard deviation of each cross section,  $\sigma$ , to the mean of each cross section,  $c_{ave}$ . Wu and Liu (2005) quantitatively characterized the mixing efficiency of their electro-kinetic micro-mixer by defining the mixing index,  $MI$  in the same way, as follows:

$$MI = \frac{\sigma}{c_{ave}} = \sqrt{\frac{1}{N-1} \sum_{i=1}^N \left( \frac{c_i - c_{ave}}{c_{ave}} \right)^2}$$

where  $N$ ,  $c_i$  and  $c_{ave}$  are the total number of pixels along line segment, the intensity at pixel  $i$ , and the average intensity over  $N$  pixels, respectively. The MI value of 1 % or less is considered as a general rule of thumb in the literature for uniform mixing (i.e., at least 99 % complete mixing). This quantity is however often problematic in judging the global mixing performance. For instance, even when a part of the total flow domain is not in a chaotic-mixing regime, the mixing index can show a high value depending on the initial distribution of the concentration (Suh, 2006). We need therefore to develop a robust quantity that represents the mixing performance both reliably and universally.

## 6. Conclusions

The micro-channel flow analysis is receiving wide attention presently, owing to its high utility potential in many multi-disciplinary applications. Often, it is required to use special numerical techniques for the analysis of flow phenomena in micro-devices. One of the important CFD tools being tried in the recent past, by researchers for the analysis of micro-channel flows includes the Lattice Boltzmann Method (LBM).

The choice of micro-structured mixers is sufficiently broad. However, there are many unresolved

issues with respect to micro-mixers which need to be addressed, presently; for instance, development of a more reliable and robust mixing quantity. There is also still room for new designs and understanding principles in this field. More robust and professional designs are needed and field trials have to be conducted to evaluate the potential in an industrial environment. Also benchmarking has to be done and the existing micro-mixers are to be categorized more scientifically.

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